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# **EUROPEAN PATENT APPLICATION**

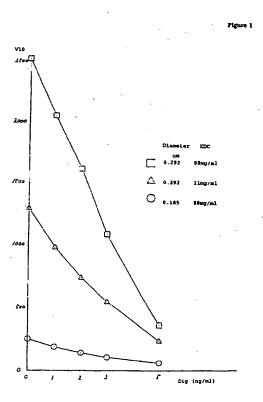
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- (54) Microparticle immunoassay reagents, sensitive and specific immunoassay reagents and immunoassay methods using these reagents.
- (57) The invention relates to sensitized carboxylate-modified latex microparticles for immunoassays having a certain diameter and parking area and immunoassay reagents that are both sensitive and specific and which require no sample pretreatment.



EP 0 679 892 A1

# Discussion of the Background

Particle-based immunoassays are well-known, and they constitute a significant portion of the immunoassay market. This is because particle-based immunoassays are highly versatile, and they may be used in tests requiring only simple visual detection and in quantitative, instrument-based analytical methods. For example, slide latex agglutination methods are known wherein an antibody or antigen is bound to latex particles and used for the detection of an antigen or antibody, respectively. In either situation, the binding of the antibody or antigen to the latex particles is typically accomplished by passive adsorption or covalent coupling.

Particle agglutination methods may be used to directly detect an antigen or an antibody (the latter being an indirect indication of the presence of an antigen). Endpoints are detected visually or instrumentally, and are chosen as either agglutination or agglutination inhibition states depending up on the specific analyte being tested. Slide tests using latex agglutination methods are typically utilized in a positive/negative qualitative format and are commonly used for infectious disease assays. Micro-particles sensitized with an immunoreactant (i.e., an antigen or an antibody) have also found use in radioimmunoassays, enzyme linked immunosorbent assays (ELISA, and membrane or particle capture-type assays.

While visual detection (agglutination, color development, etc.) is satisfactory for general screening or yes/no qualitative investigations, certain analytes require quantitative assay (drugs, haptens, etc.). Moreover, when a particle-based assay is used in high-volume screening applications (e.g., AIDS, hepatitis, etc.), it is desirable to have a fully-automated method. Particle-based instrument assays are currently being developed to meet this need. These instruments and their attendant methods are typically set up for the direct detection of an immunoreactant, optionally with multiple epitopes, or as inhibition methods for, e.g., haptens (a small molecule bound to a larger one; e.g., a drug-protein conjugate).

Several instruments and methods have been developed to quantitate immunoreactant concentration in an unknown sample by utilizing the changes occurring in light scattering caused by the specific reaction of sensitized particles with immunoreactants. Due to the large surface area of particle suspensions and the physical principles of light scattering, such methods and instrumentation can easily discriminate between signals varying from one another by from 2-3%, whereas the semi-quantitative visual evaluation methods described above have difficulty discriminating between 30-40% differences.

Immunoassay methods and devices like those described above are explained in the <u>Handbook of Experimental Immunology</u>, vols. 1-4, Blackwell Scientific 1987, incorporated herein by reference, in U.S. Patents 3,088,875, 3,857,931, 3,992,517, 4,080,264, 4,174,952, 4,203,724, 4,480,042, 4,590,156, 4,690,906, 4,716,123, 4,772,550, 4,851,329, 4,960,692 and 5,100,805, and in Grange, J. et al., <u>J. Immuno. Meth.</u>, 18,365,1977, Hechemy, K. et al., <u>Lab Management</u>, 27, June/July 1984, Looney, C., <u>J. Clin. Immunoassay</u>, 7.(1), 90, 1984, Von Schulthes, G. et al., <u>Mol Immunol</u>, 1, 81, 1980, Craine, J., <u>Am. Biotech, Lab.</u>, 34, May-June, 1987, Heveran, J., <u>J. Forensic Sci.</u>, 470, 1977 and Kimura, H. <u>J. Immuno. Meth.</u>, 38, 353, 1980, all incorporated herein by reference.

While particle-based immuoassays and sensitized (i.e., immunoreactant coated- or modified-) microparticle reagents are known, current microparticles lack the desirable characteristics of high sensitivity, good dispersibility and stability.

Digoxin is a popular cardiac glycoside currently prescribed for the control of congestive heart failure and for certain cardiac rhythm abnormalities. The increased cardiac output resulting from the inotropic action of digoxin ameliorates the disturbances characteristic of heart failure such as venous congestion, edema, dyspnea, orthopnea and cardiac asthma. Digoxin also reduces ventricular rate and thus improves hemodynamics. Palpitation, precordial distress or weakness are relieved and concomitant congestive failure ameliorated. Digoxin also slows the heart and induces regular sinus rhythm. Regardless whether digoxin is used to control/inhibit heart failure, atrial fibrillation or flutter, the cotinued administration of digoxin after the onset of clinical event is typically recommended.

The therapeutic index for digoxin is very low, there being only a very narrow difference between therapeutic and toxic dosages. Digoxin levels in patients are often difficult to predict because of variation in the absorption of oral doses and the variation and non-renal excretion. Accordingly, the monitoring of serum digoxin levels is a valuable and necessary tool in decreasing patient toxicity risk and in detecting underdigitalization. This is particularly true since the incidence of toxicity increases from 5 to 71% for serum digoxin levels of 1.1 and 4.4 mg/mL, respectively.

Current digoxin immunoassay techniques include radioimmunoassay (RIA) systems, enzyme linked immunosorbent assays (ELISA) and EMIT assays. In radioimmunoassay systems, digoxin is generally labeled with radioactive iodine and the amount of labeled digoxin bound to an antibody is measured with a gammaray counting instrument. Such RIA systems present several drawbacks, such as the use of radioactive elements, sample instability, significant reagent preparation, expensive measuring instruments, etc.

ELISA and EMIT assays also require the labeling of digoxin, albeit with an enzyme, and the subsequent monitoring of an enzyme-substrate reaction. These assay systems, like the RIA assay, require significant reagent preparation, etc. Moreover, current assays systems typically include a serum pretreatment step in order to destroy interfering proteins which contribute to non-specific (i.e., serum interferant-digoxin antibody) reactions and lead to false positive results. For example, when performing an EMIT digoxin assay, the serum or plasma is mixed with sodium hydroxide to destroy interfering proteins.

# **SUMMARY OF THE INVENTION**

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Accordingly, one object of this invention is to provide a novel immunoreactant-coated latex microparticle reagent for qualitative and quantitative immunoassays which is highly sensitive, specific and stable.

Another object of this invention is to provide a latex microparticle immunoassay reagent useful in the field of diagnostic testing, especially Toxic Drug Monitoring (TDM), and useful in latex agglutination inhibition assays.

Another object of this invention is to provide a latex-based microparticle reagent useful for the detection of cardiac glycosides and, in particular, for the detection of digoxin and digitoxin.

Another object of this invention is to provide a novel assay system which is sensitive, specific, stable and reliable and which overcomes the drawbacks of prior art assays.

Another object of this invention is provide a highly sensitive and specific digoxin assay system.

Another object of the present invention is to provide a highly sensitive and specific assay system and kit applicable to current commercial autoanalyzers useful in the field of clinical chemistry.

Another object of this invention is to provide a highly sensitive and specific cardiac glycoside assay system which can be operated without sample pre-treatment and which can be utilized to reliably determine the serum digoxin levels of patients simply and efficiently.

#### **BRIEF DESCRIPTION OF THE DRAWINGS**

A more complete appreciation of the invention and many of the attendant advantages thereof will be readily obtained as the same becomes better understood by reference to the following detailed description when considered in connection with the accompanying drawings, wherein:

Figure 1 shows the calibration curves of latex microparticle reagents according to the present invention having coupled thereto a digoxin-human serum albumin (HSA) conjugate.

Figures 2a-d show a comparison between latex-based microparticle reagents according to the present invention sensitized with either a digoxin-HSA conjugate or a digoxin-bovine serum albumin (BSA) conjugate.

Figures 3a and b show the immunoassay results of latex microparticle reagents according to the present invention sensitized with a digoxin-HSA conjugate both with and without glycine after-treatment.

Figures 4a-d show the results obtained with a present invention digoxin assay system (Y axis) as a function of the results obtained with the Abbot TDx® method (X axis).

Figure 5 shows the long term stability of the present invention digoxin sensitized microparticle reagent and antibody buffer reagent.

Figures 6a and b show the results of a digoxin assay using the LPIA-100 system using 0.296  $\mu$ m particles (Fig. 6a) and 0.434  $\mu$ m particles (Fig. 6b).

Figures 7a and b show the effects of the concentration of sodium chloride on the invention buffer reagent in a present invention digoxin assay system.

Figures 8a and 8b show the effects of the concentration of choline chloride on a digoxin assay according to the present invention.

Figures 9a-d show the effect of fatty-acid-free human serum albumin (HSA) on a digoxin assay system according to the present invention.

# DESCRIPTION OF THE PREFERRED EMBODIMENTS

The latex-based microparticle reagent according to the present invention comprises any latex-based particle which is surface carboxylate-modified and which has covalently attached thereto an immunoreactant capable of specific reaction with a complimentary immunoreactant. Preferably, the latex-based particle of the present invention has an overall diameter of from 0.020 to 0.96  $\mu$ m, preferably 0.05-0.75  $\mu$ m, more preferably 0.10-0.60  $\mu$ m, most preferably 0.18-0.5  $\mu$ m, and a 4-40, preferably 8-35, most preferably 10-30 square angstrom carboxylate surface parking area. The term "surface parking area" as used herein refers to the surface area of the latex-based microparticle measured in square angstroms divided by the total number of carboxylic

acid (-COOH) and carboxylate (-COO<sup>-</sup>) functional groups on the surface thereof. "Carboxylate" refers to both COOH and COO<sup>-</sup> functionalities. Additionally, the carboxylate-modified latex-based particles according to the invention preferably have densities ranging from 1.00 to 1.10, more preferably 1.02 to 1.06.

The latex-based particle of the present invention is any carboxylate-modified polymeric or copolymeric particle and may be made by any technique generally known in the art including emulsion polymerization, seeded emulsion . polymerization and, preferably, suspension polymerization. The particles may be made with or without a crosslinking agent and include particles of a core-shell type. Any polymeric particle having sufficient surface carboxylate groups may be used in the present invention.

Particularly useful core particles include those made from C<sub>1</sub>-C<sub>8</sub>-, preferably C<sub>1</sub>-C<sub>2</sub>-(meth)acrylates which have been carboxylate-modified, carboxylate-modified polystyrene, and a mixture of acrylic acid and styrene monomers.

Methods for preparing carboxylate-modified latex microparticles useful in the present invention are known in the art and are described in, e.g., U.S. Patents 5,015,695, 4,988,770, 4,978,719, 4,962, 154 all incorporated herein by reference.

As described above, the latex-based microparticle reagents of the present invention have a preferred diameter and a preferred carboxylate surface parking area. While the overall diameter of the invention particles may vary from 0.20-0.96  $\mu$ m, preferred diameters are from 0.1-0.6  $\mu$ m, more preferably 0.18-0.5  $\mu$ m. Particularly useful diameters include 0.20, 0.25, 0.27, 0.30, 0.35, 0.37, 0.40, 0.45 and 0.47  $\mu$ m. Further, it is preferred that the invention microparticle reagent be substantially spherical, preferably completely spherical, and it is preferred that a population of said microparticles be substantially uniform in size.

The invention microparticle reagents are carboxylate-modified and thus have free carboxylic acid and/or carboxylate moieties on the surface thereof depending upon the acidity of the medium they are or have been in contact with. The density of these acid and carboxylate residues is referred to as a surface parking area and is measured in square angstroms. The preferred parking area of the carboxylate residues for the invention microparticle reagents range from 1-35, preferably 2-30, more preferably 6-20 square angstroms. Useful parking areas include 5, 7, 10, 12, 15, 18, 20, 22, 25, 28, 30, 32 and 35 square angstroms, and, in general, 8-35 square angstrom parking areas give excellent results. The surface parking area of the invention microparticle reagents is calculated by the overall diameter and the number of acid groups, as determined by, e.g., titration, and the overall diameter of the invention microparticle reagents is measured by light scattering techniques, electron microscopy, etc.

The immunoreactant used to sensitize the invention latex microparticle reagent is any known immunoreactant capable of being covalently bonded to the surface carboxylate groups thereof. Mixtures of immunoreactants can be used, if desired. Included are hapten-carrier conjugates such as drug-protein conjugates, etc. Generally, the immunoreactants useful in the present invention are those capable of specific reaction with a complementary immunoreactant in any known immunoassay system including direct and competition assays, sandwich assays, etc.

In the present invention the term immunoreactant means any antigen or antibody optionally covalently, etc., attached to other molecules such as proteins or synthetic or natural polymers, etc., and the complementary immunoreactant means any antibody or antigen optionally covalently, etc., attached to other molecules such as synthetic or natural polymers, etc. capable of specifically binding to the immunoreactant. As used herein, the immunoreactant is the species covalently bound to the particle and the complementary immunoreactant is the specie that specifically binds thereto. Certain immunoassays, etc. may not require such an arrangement, however.

Examples of immunoreactants and complementary immunoreactants useful in the present invention include the following:

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	AFP Beta-2-microglogulin	Alpha-fetoprotein
_	CEA	Carcinoembryonic antigen
5	Ferritin	data indempi your and igen
	CA 19-9	Carbohydrate antigen 19-9
	PAP	
	PSA	Prostatic acid phosphatase
	CRP	Prostate-specific antigen
10	Mb	C-reactive protein
	RF	Myoglobin
	· · · · · · · · · · · · · · · · ·	Rheumatoid factor
	ASO	Anti-streptolysin-O
	FDP	Fibrin degradation product
	Anti-thrombin-III	•
15	Plasminogen	
	Alpha-2-plasmin inhibitor	
	D-dimer	Fibrin degradation product D-
	the second secon	fragment dimer
	IgG	Immunoglobulin G
	IgA	Immunoglobulin A
20	IgM	Immunoglobulin M
	IgE	Immunoglobulin E
	C3 ·	Complement 3
	C4	Complement 4
	Urinary albumin	combrement 4
25	hCG	Name of the state
	hPL	human chorionic gonadotropin
		Human placental lactogen
	Insulin	
	HBs antigen	Hepatitis-B surface antigen
	HBs antibody	Anti-hepatitis-B core antigen
30		antibodies
	HBc antibody	Anti-hepatitis-B core antigen
	•	antibodies
	HCV antibody	Anti-hepatitis-C virus
	•	antibodies
35	Treponema	Anti-treponema pallidum
00		antibodies
	TSH	
	LH	Thyroid stimulating hormone
	FSH	Lutenizing hormone
		Follicle stimulating hormone
40	Digoxin	

Digitoxin Quinidine Procainamide NAPA Theophylline Phenytoin Phenobarbital Carbamazepine Valproic acid Ethosuccimide Gentamicin Tobramycin Amikacin Vancomycin Cyclosporin-A **B12** Folic acid T3 **T4** Estrogen

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N-acetyl procainamide

Vitamin B12

Triiodothyronine Thyroxine

All of the above-identified species can be called either an immunoreactant or a complementary immunoreactant depending on their role in a given immunoassay. Pairing is important, the name is not, and where only an immunoreactant is referred to herein any of the above species and similar known species are meant. Naturally, all immunoreactants complimentary to those listed above are included in the present invention immunoreactants. Other immunoreactants useful in the present invention are described in the Pierce Immunotechnology Catalog and handbook, Pierce Chemical Co., 1992, incorporated herein by reference. As mentioned above, protein conjugates such as HSA and BSA conjugates of haptens are included in the invention immunoreactants. Specific examples of such carrier-hapten conjugates include digoxin-HSA and digoxin-BSA. Methods for producing these conjugates are explained in Erlanger, B. Meth. of Enzym 70, 85, 1980 and Bauminger et al., Meth. in Enzym., 70, 151, 1980, both incorporated herein by reference.

In the present invention the immunoreactant is covalently bound to the carboxylate-modified microparticle. Once the immunoreactant is bound to the microparticle, the microparticle is described as being sensitized.

The immunoreactant-coated microparticle reagent (sensitized microparticle reagent) of the present invention is prepared by covalently bonding the immunoreactant to the carboxylate-modified latex microparticle. Any method known in the art for covalently attaching immunoreactants to carboxylate groups may be used. Several techniques for the immobilization of immunoreactants on solid supports useful in the present invention are described in <a href="Immobilized Affinity Ligand Techniques">Immobilized Affinity Ligand Techniques</a>, by G. T. Hermanson, et al., 1992, in U.S. patents 4,045,384, 4,140,662 and 4,680,338, in Quasla, G. et al., J. <a href="Immuno. Meth.">Immuno. Meth.</a>, Vol. 22, 165, 1978, Srere, P. et al., <a href="Meth. Enzym.">Meth. Enzym.</a>, 44, 11, 1976, Nustad, K. et al., <a href="Devel. Biol. Stds.">Devel. Biol. Stds.</a>, 57, 321, 1984, Bahadur, A. et al., <a href="Makromol. Chem.">Makromol. Chem.</a>, 186, 1387, 1985, Margel, S. et al., <a href="J. Immuno. Meth.">J. Immuno. Meth.</a>, 28, 341, 1979, and Suen, C. et al., <a href="Makromol. Chem.">Makromol. Chem.</a>, 186, 255, 1985, all incorporated herein by reference. A linker molecule may be used.

A preferred method for covalently bonding the invention immunoreactant to the invention latex-based particle is through the use of a carbodiimide coupling reagent. The use of carbodiimide coupling reagents to effect the condensation of a carboxylic acid functionality with an amine is well-known in the art and described in <u>Organic Chemistry</u> by Streitweiser and Heathcock, MacMillan, 1976, by Sheehan, J. C., et al., in <u>J. Amer. Chem. Soc.</u> 95, 875 (1973), by Thomas, J. O., et al., in <u>J. Mol. Biol.</u>, 123, 149 (1978), by Packer, L., et al., in <u>FEBS LETT.</u>, 108, 243 (1979), in <u>Anal. Biochem.</u>, 63, 485 (1975), in <u>Plant Physiol.</u>, 53, 619 (1974), and in <u>J. Org. Chem.</u>, 21, 439 (1956), all incorporated herein by reference.

Particularly preferred carbodiimide coupling reagents for condensing the surface carboxylate groups to the immunoreactant include dicyclohexylcarbodiimide (DCC), 1-ethyl-3-(3-dimethylaminopropyl)-carbodiimide (EDC) and 1-cyclohexyl-3-(2-morpholinoethyl)carbodiimide (CMC). EDC is particularly preferred due to its high solubility, effectiveness under mild conditions and ease of reaction control. The amount of immunoreactant covalently bound to the invention particle varies depending on the particle characteristics and immunoreactant. In general, 50-10,000, preferably 200-2000 immunoreactant molecules are bound to a typical invention microparticle. However, and depending on the assay technique, desired rate of reaction, etc., this range can be altered.

Typically, the amount of carbodiimide used to effect coupling is from 0.01 to 5 percent of the weight of the particles, preferably 0.05 to 2 percent, or 2-5 times the equivalence of the latex surface carboxylate groups. See U.S. 4,181,636 and 4,045,384 incorporated herein by reference.

Carbodiimide-catalyzed coupling of carboxyl groups to amino groups can produce undesirable by-products which can provide reaction sites for non-specific reactions. In order to counter the formation of such by-products, an excess amount of an amine can be added after the coupling reaction has progressed sufficiently, and any carbodiimide-modified surface carboxylate residue can be returned to an acid or a carboxylate functionality through the use of an amino acid. In this manner, the surface charge of the invention microparticle reagent remains relatively constant and controllable. Preferred amines useful for quenching the carbodiimide coupling reaction include ethanolamine, ethylenediamine, glucosamine, glycine and lysine. Glycine and lysine are preferred, and glycine is particularly preferred.

Prior to effecting coupling of the immunoreactant to the particle it is preferred to clean the microparticle by, e.g., passing the particle through an ion exchange resin such as Bio-Rad mixed bed resin AG 501-X8.

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When an invention latex-based microparticle reagent is provided according to the present invention, high sensitivity and good dispersibility are provided. In particular, the combination of adequate particle size and relatively small surface carboxylate parking area provide a reagent particle sensitive enough to quantitate an analyte present in an amount less than 1 ng/ml. This range of sensitivity is essential for several drug monitoring applications, including digoxin assays. Further, the sensitized reagent microparticles of the present invention have excellent dispersibility in aqueous solvents and thus provide a homogeneous reagent for particle-based immunoassays yielding both reproducible results and excellent storage stability. The particular surface carboxylate parking area, particle size, etc., of the present invention reagent all make the invention reagent less susceptible to the serum matrix effect and thus improves the specificity of the reagent.

Obviously, numerous modifications and variations of the present invention are possible in light of the above teachings. It is therefore to be understood that within the scope of the appended claims, the invention may be practiced otherwise than as specifically described herein.

Furthermore, the present invention is directed to an immunoassay system and immunoassay reagents capable of determining the presence and amount of a desired species in a sample. These reagents include the above-described latex-based microparticle, and a buffer reagent comprising buffering components, sodium chloride, choline chloride, fatty-acid-free serum albumin, a polysaccharide like sodium dextransulfate or methyl cellulose, optionally a complimentary immunoreactant and, optionally, a secondary or tertiary amine non-specific reaction suppressor. Kits with two container means, one containing the above-described latex-based microparticle and the other containing the buffer components, are also provided. Any container means can be used, including vials, jars, tubes, bottles, foil packs, etc. Removably-sealed and unsealed containers can be used. The container means and sealing means can be made from any material such as glass, plastic metal, composite, etc.

The invention reagents can be used in any immunoassay system or method which utilizes the above-described latex-based microparticle which has been sensitized with an immunoreactant and a buffer reagent. Several immunoassay methods and automated and semi-automated devices in which the present invention reagents may be used are described and explained in the <a href="Handbook of Experimental Immunology">Handbook of Experimental Immunology</a>, vols. 1-4, Blackwell Scientific 1987, in U.S. Patents 3,088,875, 3,857,931, 3,992,517, 4,080,264, 4,174,952, 4,203,724, 4,480,042, 4,590,156, 4,690,906, 4,716,123, 4,772,550, 4,851,329, 4,960,692 and 5,100,805, and in Grange, J. et al., <a href="J. Immuno. Meth.">J. Immuno. Meth.</a>, 18,365,1977, Hechemy, K. et al., <a href="Lab Management">Lab Management</a>, 27 June/July 1984, Looney, C., <a href="J. Clin. Immunoassay">J. Clin. Immunoassay</a>, 7,(1), 90, 1984, Von Schulthes, G. et al., <a href="Mol Immunol">Mol Immunol</a>, 1, 81, 1980, Craine, J., <a href="Am. Biotech">Am. Biotech</a>, <a href="Lab.">Lab.</a>, 34, May-June, 1987, Heveran, J., <a href="J. Forensic Sci.">J. Forensic Sci.</a>, 470, 1977 and Kimura, H. <a href="J. Immuno. Meth.">J. Immuno. Meth.</a>, 38, 353, 1980, all incorporated herein by reference. Competitive and noncompetitive methods are included.

Preferably, a particle-based immunoassay system is utilized with the present invention immunoassay reagents, and immunoassay systems based upon latex agglutination or latex agglutination inhibition are most preferred (see U.S. 4,203,724 and 5,100,805, and <u>J. Clin. Chem.</u> 38(b), 1012 (1992), all three incorporated herein by reference). Analyzers useful for conducting immunoassays using the present invention reagents and methods include the LPIA-100 fully automated latex immunoassay system of Mitsubishi Kasei Corporation, Japan, the COBAS FARA and COBAS MIRA sytems of Roche Diagnostic Systems, Inc. and the Hitachi 704 analyzer.

When using latex particle agglutination or agglutination inhibition methods, any quantitative photometric instrument which has the capability of dispensing the sample and, optionally, an antibody reagent, into a cuvette to allow preincubation followed by the dispensing of a sensitized solid reagent into the cuvette and monitoring the ensuing reaction photometrically is preferred. Of course, any instrument capable of measuring agglutination or agglutination inhibition by, e.g., light scattering technicques, etc. can be used and sample addition, reagent addition, etc. can be conducted by hand or by semi-automated methods.

The buffer reagent of the present invention comprises buffering agents, sodium chloride, choline chloride, a polysaccharide compound such as one or both of sodium dextransulfate and methyl cellulose, optionally a complimentary immunoreactant which specifically reacts with the immunoreactant on the invention sensitized support, fatty-acid-free serum albumin and, optionally, a secondary or tertiary amine non-specific reaction suppressor.

The invention antibody buffer reagent is preferably water-based and has a pH of from 4.5 to 10, preferably 5.5 to 9.5. The amount of sodium chloride present in the buffer may vary from 1.0 to 5, preferably 1.5 to 4.5, most preferably 2.0-4.0 wt%. The amount of choline chloride present in the invention reagent buffer is from 1 to 15%, preferably 2-12%, most preferably 4-8% by weight. Typical pH buffering agents (the term "a buffering agent" means those single substances or combination of substances which resist a change in hydrogen ion concentration upon the addition of acid or alkali) are used in the present invention antibody buffer reagent. Examples include Tris-(hydroxymethyl)-aminomethane, phosphate buffering agents, those listed in the Pierce Immunotechnology Catalogue and Handbook, etc. The weight percentages above and below are based on the total buffer weight.

The present invention buffer reagent also includes at least one polysaccharide like sodium dextransulfate, methyl cellulose, etc. Other examples included carboxymethylcellulose, dextran, etc. The polysaccharide thickens the buffer reagent to an acceptable viscosity. Typically, the amount of sodium dextran sulfate useful in the present invention buffer reagent is from 0.2-3.0, preferably 0.6-2.0, most preferably 1.0-1.8 weight percent. The amount of methyl cellulose useful in the present invention buffer reagent is from 0.05-1.0, preferably 0.1-0.4, most preferably 0.15-0.3% weight percent.

The fatty-acid-free serum albumin useful in the present invention is characterized in that it is substantially free of fatty acids. The material can be prepared by the method of Chen, R.J., J. Biol. Chem., 242,173 (1967), incorporated herein by reference and may be commercially obtained in varying species and grades from Sigma and Miles. Human, bovine, rabbit, sheep, etc. serum albumins can be used. The amount of fatty-acid-free serum albumin useful in the present invention buffer is from 5-100, preferably 7.5-60, most preferably 10-40 mg/m $\ell$  of buffer. Fatty acid free human serum albumin is most preferred. Materials that are fatty acid free and globulin free are also preferred.

The optional complimentary immunoreactant useful in the present invention buffer reagent is any complimentary immunoreactant which specifically reacts with the immunoreactant used to sensitized the above-described latex-based microparticle. This species is optional since, e.g., in direct immunoassay in which the species in the sample being detected or quantitated reacts directly with the latex-based microparticle no complimentary immunoreactant in solution is necessary. When used, preferred complimentary immunoreactants are monoclonal antibodies which specifically react with the immunoreactant used to sensitized the microparticle. Anti-digoxin monoclonal antibodies are particularly preferred. Methods for producing monoclonal antibodies are well known in the art and are described in D.E. Yelton et al., <u>Annu. Rev. Biochem.</u>, 50, 657, 1981, Milstein, C., <u>Sci. American</u>, 243(4), 66, 1980; Kennett, R.H. et al. <u>Monoclonal Antibodies</u>, Plenum Press, New York, 1980 and Kohler, G. et al., <u>Nature</u>, 256, 495 (1975), all incorporated herein by reference.

As described above, an optional component of the invention buffer reagent is one or more of a secondary or tertiary amine which improves the accuracy and reliability of the invention immunoassay reagents and methods by significantly reducing or eliminating non-specific interactions. These secondary and tertiary amines may be used singly or in addmixture, and are described in copending USSN 08/194,475, incorporated herein by reference. The secondary and tertiary amine non-sepcific reaction suppressors useful in the present invention are those of the formula:

$$R_1$$
 $N-(CHY)_m-(X)_n-(CHY)_p-R_3$ 
 $R_2$ 

wherein X is -NH-(CO)-NH-, -NH-(CS)-NH-,

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or -N=C=N-,  $R_1$  and  $R_2$ , which may be the same or different, are  $C_1$ - $C_5$  linear or branched alkyl groups, or  $R_1$  and  $R_2$ , together with nitrogen, is

or the metho-p-toluenesulfonate salt thereof,

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Y, which may be the same or different, is any of H, OH and halogen (Br,  $C\ell$ , F),  $R_3$  is -NR<sub>1</sub>R<sub>2</sub>, -NH<sub>2</sub>, -CHY, cyclohexyl, or H, m is an integer of from 0 to 5, p is an integer of from 0 to 5, and n is 0 or 1,

provided that at least one of m and p is at least 1 when n equals 1, and provided that when m=n=p=0, R<sub>3</sub> is H or -CH<sub>2</sub>Y, and the acid addition salts thereof, particularly the HCl salts, phosphoric acid salts and sulfuric acid salts thereof. A preferred group of suppressors are those where m is at least 1 when n=1.

These secondary and tertiary amines may be substituted on any or all of the m and p methylenes with any combination of H, OH and halogen, include compounds where m=n=p=0 and  $R_3$  is, e.g., H or methyl, compounds where m, optionally n and optionally p are not 0 and  $R_3$  is H or -CH<sub>2</sub>Y, etc.

Several of the above-described compounds are the hydrolysis products of carbodiimides useful in the preparation of peptides. See Sheehan, J.C., et al., <u>J. Org. Chem.</u>, 26, 2525, 1961 and Staros, J.V., et al., <u>Anal. Biochem.</u>, 156, 220, 1986, both incorporated herein by reference. One particularly preferred non-specific reaction suppressor is 1-ethyl-3-(3-dimethylaminopropyl)urea (EDU), i.e., a compound according to the formula above where  $R_1=R_2=$ methyl, Y=H, y=1, y=1 and y=1, y=1

The invention non-specific reaction suppressors are generally commercially available and prepared by simple organic reactions well known to those of ordinary skill in this art and explained in, e.g., Introduction to Organic Chemistry, A. Streitwieser and C. Heathcock, Macmillan, 1976; Reagents for Organic Synthesis, Feiser and Fieser, John Wiley and Sons, 1967 and succeeding volumes; Survey of Organic Syntheses, John Wiley and Sons, Vols I and II, 1970; and Advanced Organic Chemistry, March, Wiley, 1985, all incorporated herein by reference. For example, the urea compounds (-NH-CO-NH-) can be prepared by hydrolysis of the carbodiminde (-N=C=N-) compounds.

The non-specific reaction suppressor of the present invention described by the above formula may be used singly or in combination and may be added to the invention buffer reagent or adsorbed on the above-described latex-based microparticle before or after sensitization. Further, the non-specific reaction suppressor can be utilized in combination with conventional non-specific reaction suppressors.

A particularly preferred embodiment of the present invention is one where a compound according to the above formula is used to suppress non-specific immunoassay reactions in a system in which an immunoreactant has first been bound to a solid substrate using a carbodiimide reagent such as 1-ethyl-3-(3-dimethylaminopropyl)-carbodiimide hydrochloride (EDC) or CMC. A further preferred embodiment of the present invention is one where the non-specific reaction suppressor utilized is the hydrolysis product of the carbodiimide used in the binding of the immunoreactant to the microparticle.

Wide ranges of suppressor concentration are effective. In general, the amount of non-specific reaction supressor useful for suppressing non-specific immunoassay reactions according to the invention is from 0.1 to 300 mM, preferably 0.5 to 50 mM, more preferably 1.25 to 25 mM based on the total immunoassay solution volume, the total buffer volume, the solution volume of a sample to be tested, or on the solution volume of a microparticle sensitized with immunoreactant suspended in a solvent.

The sensitized microparticle and buffer reagents of the present invention allow for highly sensitive and specific immunoassay determinations. When used in a direct-measurement (i.e., non-inhibition mode) assay the complimentary immunoreactant is omitted from the invention buffer composition, and only sodium chloride, choline chloride, polysaccharide, fatty-acid-free serum albumin and, optionally, one or more of the secondary or tertiary non-specific reaction suppressors are used with conventional buffering ingredients. When an assay based on inhibition is used a complimentary immunoreactant is present in the invention buffer reagent and the sample to be tested is contacted with the buffer reagent and incubated for from 1-20 minutes. Upon completion of incubation the sensitized microparticle is added to the mixture to bind unoccupied complimentary immunoreactant binding sights, and the rate of binding is inversely related to the immunoreactant concentration in the serum sample.

The present invention immunoassay reagents, immunoassay systems, and methods comprising them pro-

vide highly sensitive and specific determinations of specie concentration in samples, particularly patient serum samples. For example, an immunoassay system based upon latex agglutination inhibition and utilizing the preferred invention latex-based digoxin-HSA sensitized microparticle reagent and an antibody buffer reagent comprising sodium chloride, choline chloride, sodium dextransulfate or methyl cellulose, an anti-digoxin monoclonal antibody, fatty-acid-free serum albumin and e.g., 1-ethyl-3-(3-dimethyaminopropyl)-urea provides a precise and reliable assay system for determining the amount of digoxin in patient sera. This is particularly true for all the invention reagents and for the preferred reagents when the volume of the serum or plasma specimen used is less than 4% of the total immunoassay system volume, and can be accomplished without any special sample pre-treatment such as deproteination, resin treatment, ultra filtration, etc.

When the reagents of the present invention are utilized with automated, e.g., photometric, instruments commercially available and having the capability of dispensing both sample and buffer (optionally containing a complimentary immunoreactant) into a cuvette and dispensing a solid sensitized reagent into the cuvette with mixing one can quantitate the amount of sera immunoreactant for large numbers of patient samples in a short amount of time with excellent reliability and sensitivity.

The superior results afforded by the present invention reagents and immunoassay systems and methods using them (both general and preferred embodiments) are derived from several aspects of the above-described invention including the use of the fatty-acid-free serum albumin in the buffer reagent (and/or pre-applied on the sensitized microparticle if desired) and the optional use of the secondary or tertiary non-specific reaction suppressors in the buffer reagent (and/or absorbed on the sensitized microparticle, if desired). Due to the sensitivity of the present reagents and methods using them, small amounts of sample may be used while maintaining accuracy and reliability. Conventional immunoassay reagents and methods sacrifice sensitivity when sample volume is reduced: the present invention reagents and immunoassay using them maintain high sensitivity even at low sample volume.

The following examples further describe the present invention, but the invention is not limited thereto.

#### **EXAMPLES**

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# Preparation of Latex-based Microparticle

A 10 gallon glass lined reactor fitted with a condenser and stirrer was charged with 83 gms of sodium bicarbonate, 14,000 gms of deionized water and a surfactant (224 gms of MA-80). This mixture was heated to 160°F and purged with argon for 10 minutes. 208 gms of acrylic acid and 11,200 gms of styrene were mixed together and purged with argon and charged on top of the aqueous phase. The resulting emulsion was allowed to equilibrate 10 minutes.

33.6 gms of potassium persulfate was dissolved in 2000 gms deionized water, purged with argon and charged to the glass lined reactor to initiate polymerization. After 8 hours the reactor was cooled and discharged to obtain 28,000 gms of a 40% by weight suspension of 0.138  $\mu$ m carboxylate-modified microparticles. Conduct iometric titration showed 0.931 milliequivalents per gram of weak acid.

#### 40 Preparation of Digoxin Reagents

#### 1. Conjugate preparation

A digoxin-HSA conjugate was prepared according to a modified method of Smith, T. W., et al., <u>Biochemistry</u>, 9, 331 (1970) and Bulter, U.P. et al, <u>Proc. Natl. Acad. Sci. U.S.</u>, 57, 71 1967, both incorporated herein by reference. A representative protocol is as follows:

To  $0.5\,g$  of digoxin (obtained from Sigma) suspended in  $20\,ml$  of absolute ethanol at room temperature was added  $20\,ml$  of  $0.1\,M$  sodium metaperiodate dropwise with stirring. After  $25\,ml$  minutes,  $0.6\,ml$  of  $1\,M$  ethylene glycol was added. Five minutes later, the reaction mixture was added dropwise with stirring to  $0.6\,g$  of human serum albumin (obtained from Sigma) in  $20\,ml$  of  $9.5\,g$  h water (adjusted with  $10\,ml$  kgCO<sub>3</sub>). The pH of the aqueous solution was maintained in the range of from  $9.0-9.5\,g$  by the dropwise addition of  $9.6\,g$  kgCO<sub>3</sub>. After  $9.6\,g$  minutes, the pH was stable and  $9.0\,g$  of sodium borohydride freshly dissolved in  $9.0\,g$  ml of water was added thereto. Three hours later,  $9.0\,g$  ml of  $9.0\,g$  ml

2. Sensitized microparticle reagent preparation

A) Ion exchange treatment of latex particle:

To 100 ml of a carboxylate-modified latex particle suspension (10% solids;  $0.292\,\mu m$  diameter;  $0.31\,$  meq carboxylate/g, 10.5 square angstrom parking area, particle made by Seradyn, Inc. is added 20 g of a mixed-bed ion exchange resin (BioRad AG 501-X8) with slow stirring for 2 hours at room temperature. The suspension is then filtered using glass fiber filters to remove the resin, and the latex is ready for coupling.

B) Latex particle coupling reaction for digoxin-HSA conjugate:

To a 50 ml polycarbonate centrifuge tube is added 15 ml of 0.1 M bicarbonate buffer, pH 8.0, and 5 ml of the above cleaned 10% solids latex suspension, and then incubated at 37°C for 10 min with stirring prior to reaction. 5 ml of 88 mg/ml 1-ethyl-3-(3-dimethylaminopropyl)-carbodiimide hydrochloride (EDC; freshly dissolved with water) is added to the mixture to activate carboxyl residues on latex surface for 10 min. After activation, 2.5 ml of 10 mg/ml of the above digoxin-HSA conjugate is added with vigorous stirring and incubated for 10 min. The reaction is stopped by adding 5 ml of 500 mM glycine buffer, pH 8.5. Another 10 min incubation is done to ensure complete termination.

C) Washing of the conjugate coupled (i.e., sensitized) latex reagent:

The digoxin-HSA conjugate coupled latex particles are centrifuged at 26,000 x g for 20 min. The supernatant is discarded, and to the pellet is added 25 ml of water. The pellet is then resuspended by vigorous stirring and washing is repeated four times; however, in the last resuspension, 0.05% sodium azide solution is used as storage medium.

Finally, the latex suspension is sonicated and diluted to the concentration (normally 0.1-0.4% solids) ready for use.

3. Antibody reagent composition (EXAMPLE 1  $\sim$  4):

An antibody reagent is prepared by dissolving the following materials in water and adjusting the pH with hydrochloric acid. Preferably, the antibody is added last.

3.7% NaC

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200 mM Tris-(hydroxymethyl)-aminomethane, pH 8.0

1.2% Sodium Dextransulfate

1 mg/ml HSA

0.05% Sodium azide

1:60.000 diluted anti-digoxin mouse monoclonal antibody (obtained from Beekman).

4. Preparation of Anti-digoxin Antibody Buffer Reagent Composition (EXAMPLE 5 ~ 10)

A digoxin antibody reagent was prepared by dissolving the following materials in water and adjusting the pH with hydrochloric acid. The antibody was added last.

35	4.375%	NaCl
	250 mM	Bis-Tris, pH 6.5
	6.4%	Choline Chloride
40	1.25-1.75%	Sodium Dextransulfate
	2.0%	Fatty-acid-free human serum albumin
45		(FAF-HSA)
	25 mM	1-Ethyl-3-(3-dimethylaminopropyl)-
50		urea
	0.1%	Sodium azide
	0.01%	Antifoam 1410 (Dow Corning)
55	1:86,000-120,000	Diluted anti-digoxin monoclonal
		antibody

# Digoxin inhibition assay conditions and protocol (EXAMPLE 1 $\sim$ 4)

#### 1. Instrument:

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The LPIA-100® (Mitsubishi Kasei Corporation) was used for the assay.

#### 2. Assay conditions:

10 µl Specimen

50 μl Pushing buffer, 0.9% NaCl, 0.05% NaN<sub>3</sub>

200 µl Antibody reagent

40 µl Microparticle reagent

650 or 950 nm Wavelength

# 3. Assay procedure:

The digoxin assay used was based on the inhibition of the agglutination reaction between antibody and antigencoated latex particle. A serum sample containing digoxin is incubated for ten-minutes at 37°C with the anti-digoxin antibody diluted in assay buffer. Upon completion of incubation, the digoxin-coated microparticle reagent is added to bind unoccupied antibody binding sites, and the rate of agglutination is measured by the increase in absorbance at 650 or 950 nm for 10 min. The rate of increase in absorbance is inversely related to the digoxin concentration in the serum sample.

### 20 Assay Parameters for chemistry analyzers (EXAMPLE 5 ~ 10)

	Instrument name	COBAS FARA	COBAS MIRÁ	HITACHI704	LPIA100
	Wavelength	750 nm	600 nm	700 nm	650 or 950 nm
25	Temperature	37°C	37°C	37°C	37°C
	Sample volume	6 µl	6 யி	15 μl	10 µl
20	Antibody reagent	120 μ	120 µl	220 μ1	200 µl
.30	Latex reagent	25 μl	20 ய	160 μl (3x diluted)	40 µl
	Pushing water/Buffer	20 μl	35 µl	-	50 μі
35	Sample/Antibody Pre- incubation	10 min	7 min	5 min	10 min
	Reading time	5 min	4 min	5 min	10 min

# 40 EXAMPLE 1

# 1. Calibration curves of digoxin reagents

In addition to the 0.292  $\mu$ m diameter particle reagent described above, another particle reagent was made with the same particle, but using a lower concentration of EDC (11 mg/ml), and a reagent with a diameter of 0.184  $\mu$ m was prepared according to the above protocol using 88ng/ml of EDC, and all three were evaluated by measuring their digoxin calibration curves. Figure 1 shows these calibration curves made with samples having known concentrations of digoxin while measuring the rate of increase in absorbance at 650 nm with the LPIA-100 system. The curves indicate that reagents having a larger particle size have higher sensitivity (the absolute values of the rates are higher), and that all the calibration curves are satisfactory considering the therapeutic range of digoxin (0.5-2.0 ng/ml).

#### 2. Precision of 0.184 µm diameter particle reagent

According to Figure 1, the 0.184 µm sensitized particle reagent is the least sensitive. However, the reagent still has excellent performance, and provides excellent precision as is shown in Table 1.

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Table 1.

Precis	ion study usin	ig 0.184 μπ	n particle re	eagent.		
Di	Digoxin Calibrator Concentration (ng/ml)					
n=10	0.0	0.5	1.0	2.0	3.0	5.0
Rate (mA/min)						· <del>-</del>
mean	257.4	228.0	200.1	148.9	116.0	66.0
S.D.	4.3	3.8	4.0	4.3	3.6	4.3
C.V.%	1.7	1.7	2.0	2.9	3.1	6.5
Concentration calibrated						
mean	0.12	0.56	0.98	2.13	3.10	5.43
S.D.	0.06	0.06	0.07	0.12	0.15	0.20
C.V.%	-	10.0	7.5	5.6	4.8	3.7

where n is the number of samples tested, S.D. is the standard deviation and C.V.% is the coefficient of variation. The concentration calibrated refers to digoxin calibrator set (Roche Diagnostic Systems, Inc.).

# EXAMPLE 2

Fourteen different sensitized carboxylate-modified latex particles were compared in terms of their dispersibility and reactivity in the above-described digoxin inhibition assay. Microparticle reagent preparation was done based on the same preparation protocol as EXAMPLE 1. Reactivity was measured using 0 ng/ml serum calibrator as the sample.

Table 2 shows the results obtained which demonstrate the importance of adequate parking in providing reactive and dispersible microparticle reagents.

Table 2.

	Evaluation of 14 different sensitized microparticle digoxin reagents.							
5.	Sample	Diameter (μm)	Parking area (2)	g area (2) Dispersibility during:		Reactivity (mA/min) Rate		
	,			Conjugation	Assay			
0	At 650 nm	Antibody 1:400,0	00:					
•	1	0.184	18.8	Excellent	Excellent	259.6		
	2	0.203	51.9	Aggregated	Aggregated	62.1		
5	3	0.210	56.8	Clumped	Clumped	0.2		
	4	0.215	150.6	Clumped	Clumped	-0.4		
	5	0.264	34.2	Fair	Aggregated	61.1		
	6	0.283	119.7	Aggregated	Aggregated	78.6		
	7 .	0.284	16.1	Excellent	Good	1319.0		
	8	0.285	69.5	Fair	Aggregated	70.1		
	9	0.292	10.5	Excellent	Excellent	1104.2		
	10	0.296	12.0	Excellent	Excellent	1314.4		
	At 950 nm;	Antibody 1:120,0	00:					
	9	0.292	10.5	Excellent	Excellent	248.3		
	11	0.400	58.8	Aggregated	Aggregated	78.4		
	12	0.406	4.02	Excellent	Excellent	79.4		
	13	0.434	25.9	Fair	Good	763.4		
	14	0.490	2.56	Excellent	Excellent	41.8		

# **EXAMPLE 3**

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Two digoxin conjugates were prepared with bovine serum albumin (BSA) according to Smith, supra, and human serum albumin (HSA) as above. Particles were sensitized as above and were compared using the LPIA system and 50 serum specimens pre-evaluated by TDx® (Abbot). The sensitized latex particles were prepared using 0.184 µm particles according to the protocol above, and two different lots of anti-digoxin monoclonal antibody were used to make sure the results were due to the sensitized particles and not the particular antibody batch

Figures 2a and 2c show the results obtained with the latex reagents sensitized with the digoxin-BSA conjugate (black dots), the results in 2a and 2c using different antibody lots, and Figures 2b and 2d show the results of particles sensitized with digoxin-HSA using different lots of antibody (black dots).

The triangles in all Figures 2a-2d are results obtained by the LPIA-100 system using digoxin calibrators. As is seen in Figures 2a, b, c, d, the difference of antibody lot had a minimal (if any) effect on the tests, and the digoxin-HSA sensitized microparticles provided better data distribution than did digoxin-BSA sensitized particles.

# **EXAMPLE 4**

The digoxin assay described above was performed using a 0.184 μm particle sensitized with digoxin-HSA

prepared with and without glycine treatment after carbodiimide condensation reaction. In the assay, five calibrators were measured in the LPIA-100 system and 35 serum specimens were pre-evaluated by TDx® method were then tested in the LPIA-100 instrument. The results are shown as data distribution graphs together with the calibration curves in Figures 3a (without glycine after-treatment) and 3b (with glycine after-treatment).

As is shown in Figures 3a and 3b, glycine treatment reduced reactivity somewhat (i.e. lower rate values), but made sample distribution much tighter, thus improving reagent accuracy.

The invention microparticle immunoassay reagents can have adsorbed on the surface thereof, or can be provided in aqueous solutions containing, the non-specific reaction suppressors described in copending U.S. application 08/194,475, incorporated herein by reference. Kits may also be provided containing two compositions preferably in separate containers, one composition comprising the invention microparticle reagents and one composition comprising the non-specific reaction suppressors of U.S. 08/194,475.

# **EXAMPLE 5**

Patient serum specimens previously evaluated with  $TD_x$  (Abbot) for digoxin concentration were tested using the above microparticle reagent and buffer reagent in a latex agglutination inhibition assay using the four instruments described above. The data obtained with the four above-described instruments was plotted against the results obtained by the  $TD_x$  method and analyzed. Figure la shows the results obtained with COBAS FARA instrument. Figure 1b shows the results obtained with the COBAS MIRA instrument. Figure 1c shows the results obtained with the Hitachi 704 instrument. Figure 1d shows the results obtained with of LPIA-100 instrument.

As Figures 4a-d show, the latex agglutination inhibition assay conducted with reagents according to the present invention provide excellent results. The results obtained with the present invention reagents are clearly as good as, or better than, results obtained with the  $\mathsf{TD}_x$  system.

# **EXAMPLE 6**

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With the same systems described above, a precision study was conducted-using BioRad quality control serum or Roche calibrators. As shown by the data in Table 1, the present invention reagents provide far better precision than the currently accepted standard of 10% Coefficient of Variation (C.V.) at 1 ng/ml.

#### TABLE 3

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10 Day Study

3 Conc Values
n=10 Assays/Value/Day

	0.5  ng/ml		2.0 ng	2.0  ng/ml		4.0  ng/ml	
Run-to-Run:	X	CV%	<b>X</b>	CV %	X	CA#	
Day 1	0.546	7.38	1.968	4.14	3.985	2.1	
Day 2	0.542	5.97	1.939	2.95	3.973	1.5	
Day 3	0.515	4.54	1.868	2.68	3.973	1.7	
Day 4	0.493	6.01	1.869	3.25	4.038	2.5	
Day 5	0.491	8.16	1.934	3.61	, 4.103	1.1	
Day 6	0.559	5.78	2.017	3.48	4.228	2.08	
Day 7	0.581	5.18	1.957	3.89	4.034	1.19	
Day 8	0.635	6.94	2.012	1.83	4.152	3.08	
Day 9	0.634	6.71	1.987	2.89	4.092	1.04	
Day 10	0.633	6.88	1.992	3.84	4.216	1.98	
Day-to-Day	0.563	9.5	1.963	3.37	4.079	2.22	
(10 Days)	* .			•	•	•	

# **EXAMPLE 7**

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Using Seradyn's LPIA-100 system, the long term stability of the present invention reagents was evaluated. All reagents and calibrators were stored at  $4^{\circ}$ C. Measurements were conducted as follows: the serum sample and anti-digoxin antibody-containing buffer are incubated at  $37^{\circ}$  C for ten minutes. Upon completion of the incubation, a digoxin conjugated latex reagent is added to bind to unoccupied antibody binding sites. The rate of agglutination reaction is measured by the increase in absorbance at 950 nm and the reaction rate over a 5 minute absorbance measurement ( $V_{20}$ ) was plotted versus time in days in Figure 5. As shown by the results in Figure 5, the reagents were stable for at least nine months.

# **EXAMPLE 8**

Digoxin latex-based microparticle reagents having diameters of 0.296  $\mu m$  and 0.434  $\mu m$  were prepared according to the above-described protocol. 35 patient samples previously evaluated for digoxin concentration by TDx were measured in a latex-agglutination inhibition assay using the LPIA-100 system. Figures 6a-6d, where Figures 6a and 6b refer to 0.296  $\mu m$  particles and 6c and 6d refer to 0.434  $\mu m$  particles, show the results.

Figures 6a and 6c are plots of LPIA-100 rate date versus digoxin concentration as determined by DuPont ACA®; Figures 6b and 6d are plots of sample digoxin concentration of the same samples as determined by the LPIA-100 system (y axis) versus DuPont ACA®.

# **EXAMPLE 9**

A digoxin microparticle reagent was prepared according to the protocol above but having a 0.184  $\mu m$  diameter. Using the LPIA-100 instrument with a 20  $\mu m$  sample volume and the following antibody buffer system:

0.9 or 3.5%	Sodium Chloride
0 or 4%	Coline Chloride
200 mM	Tris-(hydroxmethyl)amino methane, pH 7.5
1.2-1.3%	Sodium Dextransulfate
1 mg/ml bovine	Serum albumin
0.05%	Sodium azide
1:40,000	Diluted anti-digoxin-monoclonal antibody

30 patient samples were evaluated for digoxin concentration. Figures 7a and 7b show the results obtained with 0.9 and 3.5% sodium chloride, respectively (using 0% choline chloride), and Figures 8a and 8b show the result obtained with 0 and 4% choline chloride, respectively, using 3.5% sodium chloride.

# **EXAMPLE 10**

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A digoxin-sensitized microparticle reagent was prepared according to the above protocol but having a diameter of 0.292 μm and 35 patient samples were evaluated with the LPIA-100 system using 10 μl sample volumes. The antibody buffer composition used was follows:

3.5%	Sodium Chloride
250 mM	Sodium acetate, pH 5.5-7.5
0.16%	Methyl cellulose
0.1-4%	Fatty-acid-free-HSA
250 mM	1-ethyl-3-(3-dimethyl-aminopropyl-urea)
0.05%	Sodium azide
1:60,000	Diluted anti-digoxin-monoclonal antibody

The results are presented in Figures 9 a-d where 9a is a control using 1.25 mg/ml FAF-HSA and with Figures 9b, 9c and 9d using 10, 20 and 40 mg/ml of FAF-HSA respectively.

### Claims

- 2. The microparticle of Claim 1, wherein said particle has a diameter of from 0.18-0.5 μm.
  - 3. The microparticle of Claim 2, wherein said particle has a parking area of from 10-30 square angstroms.
- 4. The microparticle of Claim 1, wherein said immunoreactant is a hapten-protein conjugate.
  - 5. The microparticle of Claim 4, wherein said immunoreactant is a digoxin-protein conjugate.
  - 6. The microparticle of Claim 3, wherein said immunoreactant is a digoxin-human serum albumin conjugate.
- 7. The microparticle of Claim 1, wherein said immunoreactant is covalently bound to said carboxylate-modified latex particle in a condensation reaction in the presence of a carbodiimide.

- The microparticle of Claim 7, wherein said carbodiimide is 1-ethyl-3-(3-dimethylaminopropyl)carbodiimide hydrochloride.
- 9. The microparticle of Claim 7, wherein said condensation reaction is stopped with a compound selectded from the group consisting of ethanolamine, ethylenediamine, glucoseamine, glycine and lysine.
- 10. The microparticle of Claim 7 wherein said condensation reaction is stopped with glycine.
- A particle-based immunoassay method comprising contacting the sensitized microparticle of Claim 1 with a complementary immunoreactant.
- 12. A kit comprising two components A and B, component A comprising the microparticle of Claim 1, component B comprising a buffer composition comprising a buffering agent, sodium chloride, choline chloride, a polysaccharide and fatty-acid-free serum albumin.
- 13. The kit of Claim 12, wherein said buffer composition further comprises a non-specific reaction suppressor of the formura:

$$R_1$$
 $N-(CHY)_m-(X)_n-(CHY)_p-R_3$ 

wherein X is -NH-(CO)-NH-, -NH-(CS)-NH-,

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or -N=C=N-,  $R_1$  and  $R_2$ , which may be the same or different, are  $C_1$ - $C_5$  linear or branched alkyl groups, or  $R_1$  and  $R_2$ , together with nitrogen, is

or the metho-p-toluenesulfonate salt thereof,

Y, which may be the same or different, is any of H, OH and halogen,

R<sub>3</sub> is -NR<sub>1</sub>R<sub>2</sub>, -NH<sub>2</sub>, -CHY, cyclohexyl, or H,

m is an integer of from 0 to 5,

p is an integer of from 0 to 5, and

n is 0 or 1,

provided that at least one of m and p is at least 1 when n equals 1, and provided that when m=n=p=0,  $R_3$  is H or -CH<sub>2</sub>Y, and the acid addition salts thereof.

- 14. The kit of Claim 13, wherein said non-specific reaction suppressor is 1-ethyl-3-(3-dimethylaminopropyl)-urea.
- 15. The kit of Claim 12, wherein said buffer composition further comprises water, 1.0-5.0% by wt. sodium chloride, 1-15% by weight choline chloride, 0.2-0.3% by weight sodium dextransulfate or 0.05-1.0% by weight methyl cellulose, said percentages by wt. based on the total weight of the buffer, and 5-100 mg/ml of fatty-acid-free human serum albumin based on the total volume of the buffer.
- 16. The kit of Claim 15, wherein said buffer further comprises a complementary immunoreactant.
- 17. The kit according to Claim 16, wherein said complimentary immunoreactant is an anti-digoxin monoclonal

antibody.

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18. An immunoassay method comprising the steps of:

mixing a sample comprising an analyte to be detected with a buffer composition comprising water, a buffering agent, sodium chloride, choline chloride, a polysaccharide, fatty-acid-free serum albumin, and, optionally, a non-specific reaction suppressor of the formula:

$$R_1$$
 $N-(CHY)_m-(X)_n-(CHY)_p-R_3$ 

wherein X is -NH-(CO)-NH-, -NH-(CS)-NH-,

or -N=C=N-,  $R_1$  and  $R_2$ , which may be the same or different, are  $C_1$ - $C_5$  linear or branched alkyl groups, or  $R_1$  and  $R_2$ , together with nitrogen, is

0 N-

or the metho-p-toluenesulfonate salt thereof,

Y, which may be the same or different, is any of H, OH and halogen,

R<sub>3</sub> is -NR<sub>1</sub>R<sub>2</sub>, -NH<sub>2</sub>, -CHY, cyclohexyl, or H, m is an integer of from 0 to 5, p is an integer of from 0 to 5, and n is 0 or 1.

provided that at least one of m and p is at least 1 when n equals 1, and provided that when m=n=p=0, R<sub>3</sub> is H or -CH<sub>2</sub>Y, and the acid addition salts thereof to produce a buffer-sample mixture, and contacting said buffer-sample mixture with the microparticle of Claim 1.

- 19. The method of Claim 18, wherein said buffer further comprises a complimentary immunoreactant.
- 20. The method of Claim 18, wherein said buffer composition comprises 1.0-5.0% by wt. sodium chloride, 1-15% by weight choline chloride, 0.2-3.0% by weight sodium dextransulfate or 0.05-1.0% by weight methyl cellulose, said percentages by wt. based on the total weight of the buffer, and 5-100 mg/ml of fatty-acid-free human serum albumin based on the total volume of the buffer.
- 21. The method of Claim 19, wherein said buffer composition comprises 1.5-4.5%-by wt. sodium chloride, 2-12% by weight choline chloride, 0.6-2.0% by weight sodium dextransulfate or 0.1-0.4% by weight methyl cellulose, said percentages by wt. based on the total weight of the buffer, and 60-75 mg/ml of fatty-acid-free human serum albumin.

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Figure 1

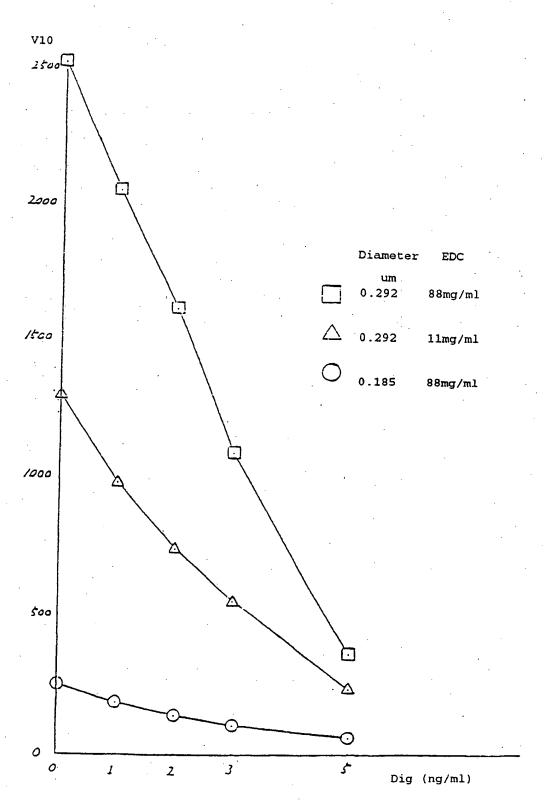


Figure 2

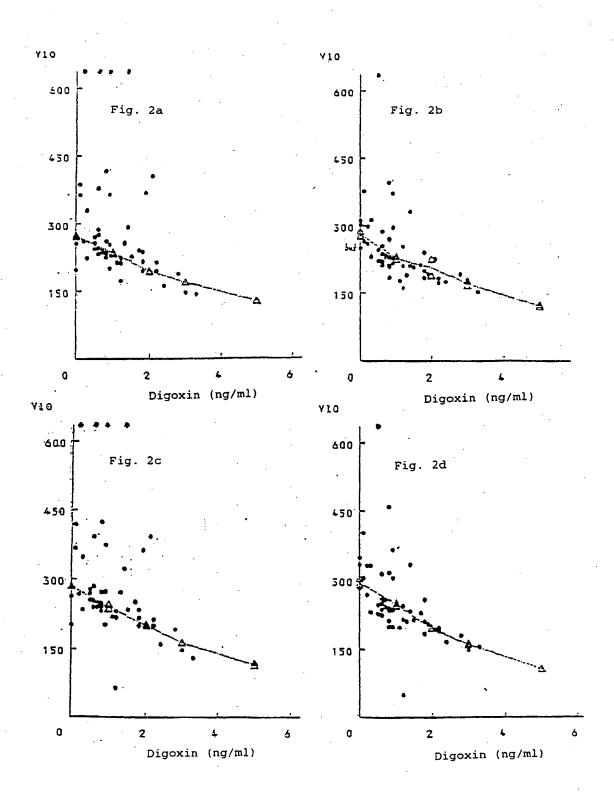
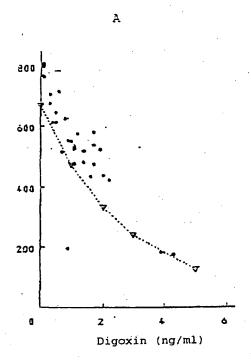
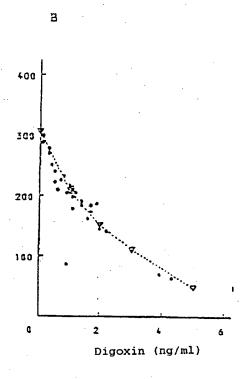


Figure 3



without glycine



with glycine

Figure 4A

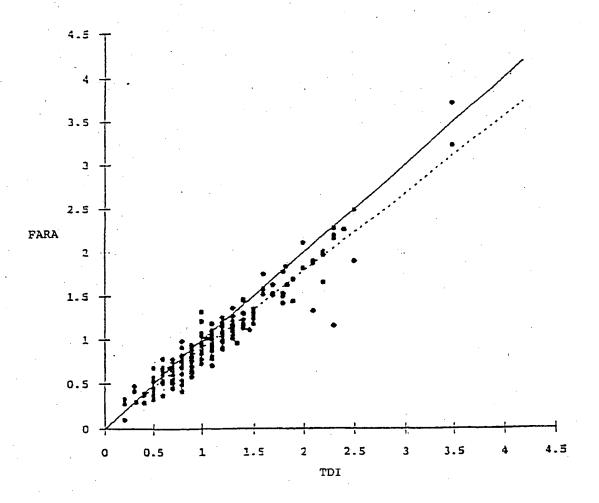


Figure 4B

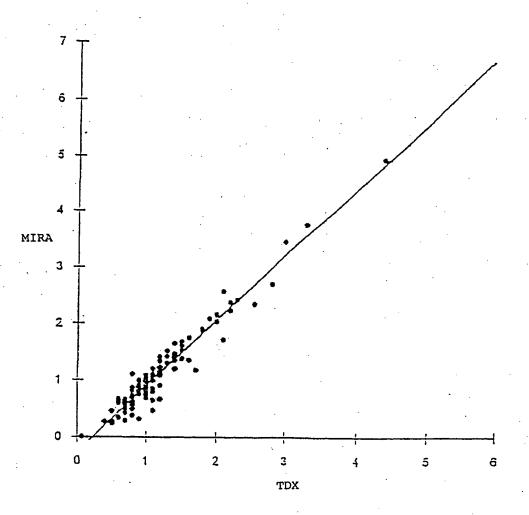


Figure 4C

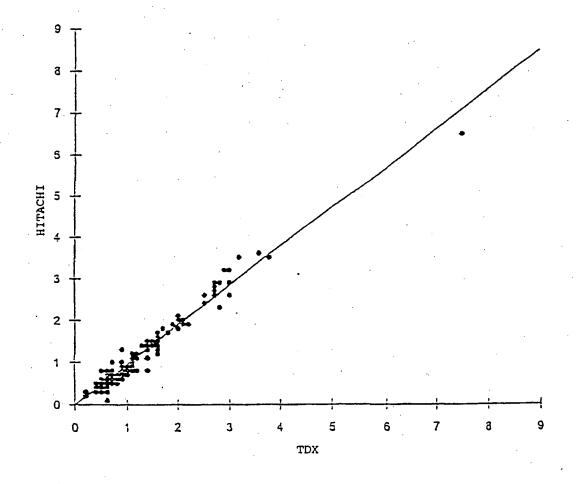
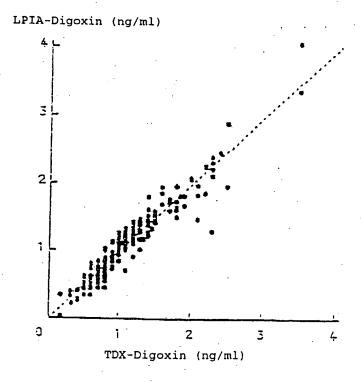


Figure 4D





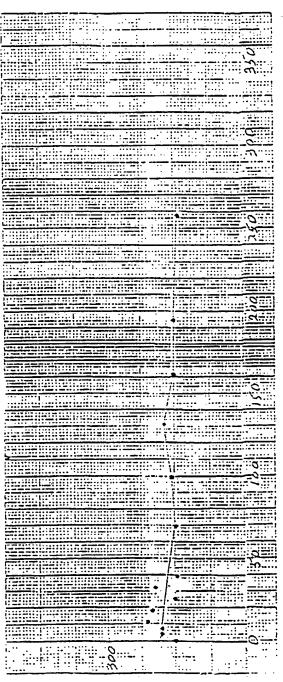


Figure 6

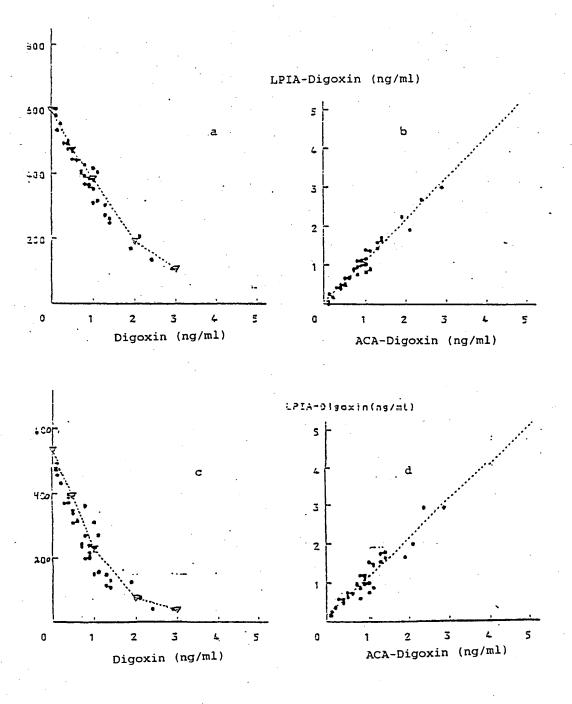


Figure 7

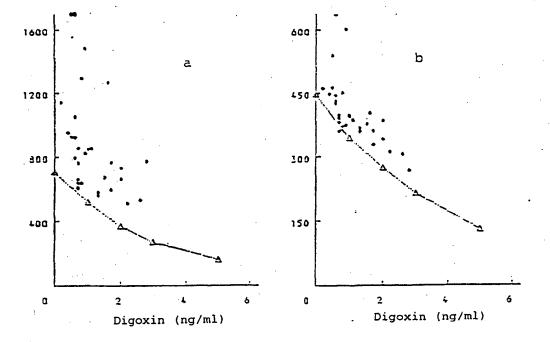
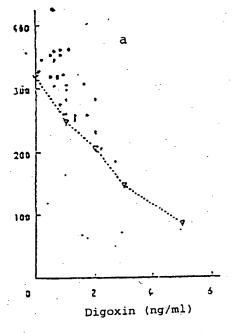


Figure 8



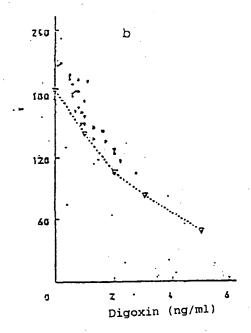
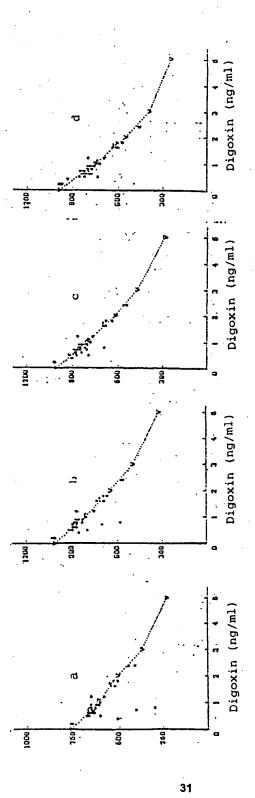


Figure 9





# EUROPEAN SEARCH REPORT

Application Number

	OCUMENTS CONSIDERED TO		<del></del>	EP 95106506.9
ategory	Citation of document with indication, where of relevant passages	apprepriate,	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IBL CL 6)
A .	<u>US - A - 5 302 532</u> (LAU) * Claims 1,4,5,7; example 3 *		1-11, 18-21	G 01 N 33/546
4	WO - A - 90/08 321 (DIAGNOSTICA STAGO) * Abstract *		1-11, 18-21	
		· ·		
				TECHNICAL FIELDS SEARCHED (Int. Cl.6)
				G 01 N 33/00
	•			
		of completion of the search  6-1995		Examples SCHNASS
X : partic Y : partic	ATEGORY OF CITED DOCUMENTS  ularly relevant if taken alone ularly relevant if combined with another nent of the same category	T: theory or princ E: earlier patent d after the filing D: document cited L: document cited	iple underlying the comment, but pur date	he invention blished on, or